Package 'oro.pet'

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Description Image analysis techniques for positron emission tomography (PET) that form part of the Rigorous Analytics bundle.

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R topics documented:

.petWrapper 2
activityConcentration 2
compartmentalModel 4
expConv 5
hillEquation 5
leanBodyMass 7
multilinearReferenceTissueModel 8
occupancy 10
plotBindingPotential 11
simplifiedReferenceTissueModel 12

Index **14**

`.petWrapper` *Wrapper for oro.pet functions*

Description

Simple wrapper for getting functions from

Usage

```
.petWrapper(name, ...)
```

Arguments

`name`	name of function (without leading ".")
`...`	Additional arguments passed to `oro.nifti::.wrapper`

`activityConcentration` *Calculating SUVs for PET Using QIBA Pseudocode*

Description

The standard uptake value (SUV) is calculated based on an 18F-FDG-PET acquisition using ancillary information contained in the DICOM data.

Usage

```
activityConcentration(pixelData, ...)

## S4 method for signature 'array'
activityConcentration(pixelData, CSV = NULL,
  seriesNumber = NULL, method = "qiba")

.activityConcentration(pixelData, CSV = NULL, seriesNumber = NULL,
  method = "qiba")

standardUptakeValue(pixelData, ...)

## S4 method for signature 'array'
standardUptakeValue(pixelData, mask = NULL, CSV = NULL,
  seriesNumber = NULL, method = c("qiba", "user"), prior = NULL,
  decayedDose = NULL)

.standardUptakeValue(pixelData, mask = NULL, CSV = NULL,
  seriesNumber = NULL, method = c("qiba", "user"), prior = NULL,
  decayedDose = NULL)
```

Arguments

pixelData	is a multidimensional array of signal intensities of class nifti.
...	additional arguments
CSV	is a data.frame that is the output from dicomTable and contains all necessary DICOM header fields.
seriesNumber	is the SeriesNumber that corresponds to the PET acquisition.
method	takes on two possible values (qiba and user), where QIBA pseudocode is used to calculate the SUVs or user-defined parameters are used.
mask	is a multidimensional array of logical values (only used when method = "user").
prior	is a list of DICOM header field names that are necessary for the SUV calculation under method = "user" or may be used to replace values from the DICOM header information when method = "qiba".
decayedDose	is the amount of the RadionuclideTotalDose after being corrected for residual dose in the syringe. This value is NOT usually corrected in the DICOM data.

Value

A list containing the following items

- SUVbwis a multidimensional array, the same dimension as pixelData, that contains the standard uptake values.
- hdris a list of DICOM header fields used in the SUV calculation.
- decayTimeis the decay time calculated from the DICOM header information.
- decayedDoseis the RadionuclideTotalDose, if taken from the DICOM header information, or the user-specified value.
- SUVbwScaleFactoris PatientsWeight $\cdot$ $1000/$decayedDose.

Note

Note, for GE scanners it is common for the RescaleSlope DICOM field to vary on a slice-by-slice basis. This is taken into account if a GE scanner is detected from the Modality DICOM field. However, the InstanceNumber is used to reorder the slices so they match the incoming NIfTI file of PixelData. If this is not correct it may be necessary to manually re-order the RescaleSlope field in the CSV data frame so that the activity concentration is calculated correctly.

Author(s)

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References

http://qibawiki.rsna.org/index.php?title=Standardized_Uptake_Value_(SUV)

See Also

dicomTable, nifti

`compartmentalModel` *Compartmental Models for Kinetic Parameter Estimation*

Description

A selection of parametric models are provided that combine a compartmental model for tissue and empirical versions of the arterial input function or reference region time activity curve.

Usage

```
compartmentalModel(type)
```

Arguments

`type`	is a character string that identifies the type of compartmental model to be used. Acceptable models include:
	list("srtm") Simplified Reference Tissue Model
	list("srtm2") Simplified Reference Tissue Model in two steps

Details

Parametric models from the PET literature are provided to the user for kinetic parameter estimation.

Value

A function.

Author(s)

Brandon Whitcher <bwhitcher@gmail.com>

References

Lammertsma, A.A and Hume, S.P. (1996) Simplified reference tissue model for PET receptor studies, *NeuroImage*, **4**, 153-158.

Wu, Y and Carson, R.E. (2002) Noise reduction in the simplified reference tissue model for neuroreceptor functional imaging, *Journal of Cerebral Blood Flow \& Metabolism*, **22**, 1440-1452.

See Also

`simplifiedReferenceTissueModel`

expConv — *Empirical Convolution Between an Input Function and a Single Exponential*

Description

Computationally efficient method to convolve a vector of observations and a single exponential function with two parameters.

Usage

```
expConv(input, k1, k2)
```

Arguments

input	is the so-called input function.
k1	is the scaling parameter in the single exponential function.
k2	is the decay parameters in the single exponential function.

Details

Assuming the input function has been sampled (or interpolated) to a high temporal resolutions, say one Hertz, a simple for loop is used to perform the convolution.

Value

The vector containing the result from the convolution operation.

Author(s)

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hillEquation — *Estimation of the Half Maximal Inhibitory Concentration*

Description

The half maximal inhibitory concentration (IC50) is a measure of the effectiveness of a compound in inhibiting biological or biochemical function. This quantitative measure indicates how much of a particular drug or other substance (inhibitor) is needed to inhibit a given biological process (or component of a process) by half.

See reference(s).

In this version of the function the maximal occupancy (rmax) is estimated automatically. This should be optional.

Usage

```
hillEquation(conc, occ, guess = c(1, 100),
  control = minpack.lm::nls.lm.control())
```

Arguments

conc	a vector of drug concentrations in plasma (example units are ng/mL).
occ	a vector of PET occupancy values that correspond to the measured drug concentrations in plasma.
guess	a length-two vector of starting values for the nonlinear optimization.
control	is a list of parameters used by nls.lm.control that are set by default, but may be customized by the user.

Value

List with the following elements

- IC50Half maximal inhibitory concentration
- rmaxEstimated maximal occupancy
- IC50SEApproximate standard error for IC50
- rmaxSEApproximate standard error for rmax
- hessianHessian matrix from the Levenburg-Marquardt procedure
- infoReturn value from the Levenburg-Marquardt procedure
- devianceDeviance from the Levenburg-Marquardt procedure
- messageText message from the Levenburg-Marquardt procedure

Author(s)

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References

Hill Equation IC50

See Also

nls.lm

leanBodyMass *Calculating the Lean Body Mass*

Description

The lean body mass (LBM) is calculated according to the formula

$$1.1 \cdot \text{weight} - 128 \cdot (\text{weight}/\text{height})^2$$

if male and

$$1.07 \cdot \text{weight} - 148 \cdot (\text{weight}/\text{height})^2$$

if female.

Usage

```
leanBodyMass(height, weight, gender)

hotSpotSUV(suv, radius = 10, type = "3D")

totalSUV(suv, mask, z, bg, local = TRUE)
```

Arguments

height	is a vector of heights in centimeters.
weight	is a vector of weights in kilograms.
gender	is a character vector (may be of length one) with the value "male" or "female".
suv	is the standard uptake value (SUV).
radius	is the desired hotspot radius (units = voxels).
type	is a character string (acceptable values are 2D or 3D) that determines the dimension of the hot spot (default = 3D).
mask	is a multidimensional array of logical values.
z	is the slice index.
bg	is the estimated background SUV.
local	is a logical value.

Value

Vector of lean body mass values in kilograms.

...

Author(s)

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References

Sugawara, Y., K. R. Zasadny, A. W. Neuhoff, R. L. Wahl (1999) Reevaluation of the Standardized Uptake Value for FDG: Variations with Body Weight and Methods for Correction, *Radiology* **213**: 521–525.

See Also

standardUptakeValue

leanBodyMass

Examples

```
library(oro.pet)
n <- 11
h <- seq(200, 150, length=n)
w <- seq(80, 120, length=n)
cbind(h, w, leanBodyMass(h, w, "male"), leanBodyMass(h, w, "female"))
```

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multilinearReferenceTissueModel

The Multilinear Reference Tissue Model

Description

The multilinear reference tissue model (MRTM) estimates the binding potential from an observed time activity curve without the need for arterial sampling. Instead, a second time activity curve must be provided from a suitable reference region where there is negligible binding.

Usage

```
multilinearReferenceTissueModel(tac, ref, time, tstar, MRTM2 = TRUE,
  k2prime = NULL)
```

Arguments

tac	a vector corresponding to the time activity curve from the tissue (in Bq/mL).
ref	a vector corresponding to the time activity curve from the reference region (in Bq/mL).
time	a vector of average frame times (in minutes).
tstar	the time (in minutes) where the linear relationship between the response and covariates may be assumed to be true.
MRTM2	a logical value that selects the three-parameter model (MRTM) or the two-parameter model (MRTM2), where k2prime is fixed.
k2prime	the value of k2prime that has been fixed.

Details

See the references.

The numeric integration required to construct the design matrix is performed by interpolating the time activity curves, both for the tissue and reference region, to one-second resolution and then performing the `cumsum` operation on them.

Given the nonlinear relationship between binding potential and the regression parameters, the `deltamethod` is used to approximate its standard error.

Value

`BP`	Binding potential
`BP.error`	Approximate standard error of the binding potential
`R1`	Ratio of the volumes of distrubution for the tissue and reference region (assumes a one-tissue model is valid)
`R1.error`	Approximate standard error for the ratio
`k2`	Clearance rate constant from the tissue to plasma (assumes a one-tissue model is valid)
`k2.error`	Approximate standard error for k2
`X`	Design matrix used in the linear regression
`beta`	Regression coefficients

Author(s)

Brandon Whitcher `<bwhitcher@gmail.com>`

References

Ichise, M., Ballinger, J.R., Golan, H., Vines, D., Luong, A., Tsai, S. and Kung, H.F. (1996) Non-invasive quantification of dopamine D2 receptors with iodine-123-IBF SPECT, *Journal of Nuclear Medicine*, **37**, 513-520.

Ichise, M., Liow, J.-S., Lu, J.-Q., Takano, A., Model, K., Toyama, H., Suhara, T., Suzuki, K., Innis, R.B., Carson, R.E. (2003) Linearized reference tissue parametric imaging methods: Application to [11C]DASB positron emission tomography studies of the serotonin transporter in human brain, *Journal of Cerebral Blood Flow \& Metabolism*, **23**, 1096-1112.

See Also

`cumsum`, `deltamethod`

occupancy *Compute Drug Occupancy with Approximate Standard Errors*

Description

Receptor occupancy is calculated from positron emission tomography (PET) data as the treatment-induced relative change in the concentration of available (not occupied) receptors.

Usage

```
occupancy(base, drug, baseSE = NULL, drugSE = NULL, base.drug.corr = 0)
```

Arguments

base	is the baseline binding potential (BPND).
drug	is the post-treatment binding potential (BPND).
baseSE	is the standard error for the baseline BPND.
drugSE	is the standard error for the post-treatment BPND.
base.drug.corr	is the user-specified correlation between baseline and post-treatment binding potentials.

Details

Occupancy is calculated using the straightforward and well-known formula. If the standard errors for the two binding potentials are provided, then the delta method is used to approximate the standard error for the estimate of occupancy.

Value

OCC	is the percent drug occupancy.
SE	is the approximate standard error of the parameter estimate.

Author(s)

Brandon Whitcher <bwhitcher@gmail.com>

References

Cunningham VJ, Rabiner EA, Slifstein M, Laruelle M (2010). Measuring drug occupancy in the absence of a reference region: the Lassen plot re-visited, *Journal of Cerebral Blood Flow & Metabolism*, **30**, 46-50.

Passchier J, Gee A, Willemsen A, Vaalburg W, van Waarde A (2002). Measuring drug-related receptor occupancy with positron emission tomography, *Methods*, **27**, 278-286.

See Also

deltamethod

plotBindingPotential *Plot Baseline Versus Post-Treatment Binding Potentials*

Description

Inspired by the Lassen plot (Cunningham et al., 2010) this is a straightforward graphical summary of pre-treatment versus post-treatment binding potentials for a single subject across multiple brain regions.

Usage

```
plotBindingPotential(base, drug, lty45 = 2, lty = 1, lwd45 = 2, lwd = 3,
  col45 = "darkgrey", col = "orange", pch = 1, cex = 1,
  xlim = range(0, base, 0.5), ylim = range(0, drug, 0.5),
  xlab = expression(BP[ND]^{     Base }), ylab = expression(BP[ND]^{
  Drug }), ...)
```

Arguments

base	is the vector of baseline binding potentials across brain regions.
drug	is the vector of post-treatment binding potentials across brain regions.
lty45	is the line type for the 45-degree line.
lty	is the line type for the estimated regression line.
lwd45	is the line width for the 45-degree line.
lwd	is the line width for the estimated regression line.
col45	is the color for the 45-degree line.
col	is the color for the estimated regression line.
pch	is the plotting character symbol.
cex	is the size of the plotting symbol.
xlim	is the range of values on the x-axis.
ylim	is the range of values on the y-axis.
xlab	is the label on the x-axis.
ylab	is the label on the y-axis.
...	additional arguments to be passed to the plot function.

Details

See the reference below.

Value

A plot is shown, NULL is returned

Author(s)

Brandon Whitcher <bwhitcher@gmail.com>

References

Cunningham VJ, Rabiner EA, Slifstein M, Laruelle M (2010). Measuring drug occupancy in the absence of a reference region: the Lassen plot re-visited, *Journal of Cerebral Blood Flow & Metabolism*, **30**, 46-50.

See Also

par, plot

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simplifiedReferenceTissueModel

The Simplified Reference Tissue Model

Description

The simplified reference tissue model (SRTM) estimates the binding potential from an observed time activity curve without the need for aterial sampling. It assumes a one-tissue compartment model to describe the influx and efflux in the tissue region of interest and the reference region.

Usage

```
simplifiedReferenceTissueModel(tac, ref, time, SRTM2 = TRUE, k2prime = NULL,
  guess = c(R1 = 0.5, k2 = 0.01), control = minpack.lm::nls.lm.control())
```

Arguments

tac	a vector corresponding to the time activity curve from the tissue (in Bq/mL).
ref	a vector corresponding to the time activity curve from the reference region (in Bq/mL).
time	a vector of average frame times (in minutes).
SRTM2	a logical value that selects the three-parameter model (SRTM) or the two-parameter model (SRTM2), where k2prime is fixed.
k2prime	the value of k2prime that has been fixed.
guess	values for the initial parameter estimates for R1 and k2.
control	a list of parameters used by nls.lm.control that are set by default, but may be customized by the user.

Details

See the references.

The model has been parameterized in the manner of Wu and Carson (2002). That is, the nonlinear regression estimates R1, k2 and k'2 for the three-parameter model (SRTM) and R1 and k2 for the two-parameter model (SRTM2).

The convolution is performed after interpolating the time activity curves, both for the tissue and the reference region, to one-second resolution then downsampling them back to the original sampling rate.

Value

`BP`	Binding potential
`R1`	Ratio of the volumes of distrubution for the tissue and reference region
`k2`	Clearance rate constant from the tissue to plasma
`BP.error`	Approximate standard error of the binding potential
`R1.error`	Approximate standard error for the ratio
`k2.error`	Approximate standard error for k2

Author(s)

Brandon Whitcher <b.whitcher@gmail.com>

References

Lammertsma, A.A. and Hume, S.P. (1996) Simplified reference tissue model for PET receptor studies, *NeuroImage*, **4**, 153-158.

Wu, Y. and Carson, R.E. (2002) Noise reduction in the simplified reference tissue model for neuroreceptor functional imaging, *Journal of Cerebral Blood Flow \& Metabolism*, **22**, 1440-1452.

See Also

`deltamethod`, `expConv`, `nls.lm`

Index

∗Topic **misc**
    compartmentalModel, 4
    expConv, 5
.activityConcentration
        *(*activityConcentration*)*, 2
.petWrapper, 2
.standardUptakeValue
        *(*activityConcentration*)*, 2

activityConcentration, 2
activityConcentration,array-method
        *(*activityConcentration*)*, 2

compartmentalModel, 4
cumsum, *9*

deltamethod, *9, 10*, *13*
dicomTable, *3*

expConv, 5, *13*

hillEquation, 5
hotSpotSUV *(*leanBodyMass*)*, 7

leanBodyMass, 7, *8*

multilinearReferenceTissueModel, 8

nifti, *3*
nls.lm, *6*, *13*

occupancy, 10

par, *12*
plot, *12*
plotBindingPotential, 11

simplifiedReferenceTissueModel, *4*, 12
standardUptakeValue, *8*
standardUptakeValue
        *(*activityConcentration*)*, 2
standardUptakeValue,array-method
        *(*activityConcentration*)*, 2
Summarizing SUVs *(*leanBodyMass*)*, 7

totalSUV *(*leanBodyMass*)*, 7